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(54) Title: **BIOCOPATIBLE METALLIC STENTS WITH HYDROXY METHACRYLATE COATING**  
(54) Titre: **STENT METALLIQUE BIOCOPATIBLE A REVETEMENT D'HYDROXYMETHACRYLATE**

## (57) Abstract

The invention provides a hemo-compatible, restenosis-inhibiting metallic stent, comprising a coating of a poly-hydroxy methacrylate derivate selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof.

## (57) Abrégé

L'invention concerne un stent métallique hémocompatible, inhibant la resténose, comprenant un revêtement de polyhydroxyméthacrylate sélectionné dans le groupe comprenant le polyhydroxyéthyl méthacrylate (PHEMA), le poly(hydroxyéthoxyéthyl méthacrylate) (PHEEMA), le poly(hydroxydiéthoxyéthyl méthacrylate) (PHDEEMA), le poly(méthoxyéthyl méthacrylate) (PMEMA), le poly(méthoxyéthoxyéthyl méthacrylate) (PMEEMA), le poly(méthoxydiéthoxyéthyl méthacrylate) (PMDEEMA), le poly(éthylèneglycol diméthacrylate) (PEGDMA), ainsi que des mélanges de ces composés.

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(54) Title: BIOCOMPATIBLE METALLIC STENTS WITH HYDROXY METHACRYLATE COATING			
(57) Abstract			
<p>The invention provides a hemo-compatible, restenosis-inhibiting metallic stent, comprising a coating of a poly-hydroxy methacrylate derivate selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof.</p>			

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**Description**

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## BIOCOMPATIBLE METALLIC STENTS WITH HYDROXY METHACRYLATE COATING

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**Technical Field**

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The present invention relates to the application of a coating of a poly-hydroxymethacrylate derivative to improve the biocompatibility of metal stents intended for implantation or insertion. More specifically, the present invention relates to the coating of metallic stents with effective amounts of a coating of a poly-hydroxymethacrylate derivative which will drastically increase the thromboresistance of the stent, as well as prevent any significant deposit of protein, or the occurrence of mineral encrustation, and thereby achieve inhibition of restenosis.

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**Background Art**

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Advances in medical and surgical technology involving the introduction of implantation of foreign materials, such as stents, catheters, prostheses, etc. into body-tissue make the search for the development of materials that exhibit a long-term biocompatibility more pressing than ever before. A wide range of materials and polymers have been tested and used in medical device applications. These include polyethylene, polypropylene, polyvinylchloride, polyesters, polystyrene, polyurethane, silicone, polysulphone, polyamide, polytetrafluoroethylene, cellulose and its derivatives. Although they have excellent mechanical and physical properties, they were originally developed for the use in industrial manufacturing and not specifically for the biomedical field.

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Foremost among the difficulties that need to be addressed within a medical or surgical context are the problems concerning the development of thromboresistant materials and coatings that will resist protein deposits and adverse vessel-wall reactions. Indeed, it is by now well-documented that adverse reactions between foreign or prosthetic surface and blood components, e.g. platelet-activation and thrombogenesis, constitute the single most important factor limiting the use of certain biomaterials. To prevent uncontrolled hemostasis, patients need to be

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10 treated prophylactically with anti-coagulants, such as heparin or warfarin. In a  
considerable fraction of these cases, depending on the site of deployment of the  
implant, the patient needs to continue this medication indefinitely, necessitating a  
strictly controlled regime of drug-taking which effectively balances the patient on a  
narrow operational strip flanked by the dual dangers of uncontrolled bleeding on  
the one hand and the development of an embolism on the other, both obviously  
15 equally disastrous outcomes. Even if this treatment can be discontinued after a  
limited period of time, it complicates the procedure and significantly increases the  
patient's risk of post-operative bleeding and infection.

20 As a matter of fact, some biomedical applications are totally precluded by the  
thrombogenic potential of stents and/or synthetic polymers. An example of this is  
25 the small diameter vascular graft for use in coronary artery bypass. At present, all  
synthetic materials fail in this application and a patient requiring coronary bypass  
must first undergo a procedure to remove the saphenous vein from the leg. This  
vein is subsequently used to carry out the bypass itself. A biocompatible material  
30 would have an enormous benefit in this application.

35 With regard to the problem of protein deposition, this manifests itself whenever  
biological fluids come into contact with synthetic surfaces such as glass, steel or  
polymers. These deposits have an important impact on the course of subsequent  
events occurring at the surface such as platelet adhesion-activation for blood  
containing devices, or mineral encrustation on urological stents. The risk of  
40 thrombus formation is, in the case of some devices, also accompanied by the  
additional risk of infection as a result of the adhesion and proliferation of bacteria at  
the surface of a biomaterial.

45 Numerous experiments have been conducted aiming at improving the  
biocompatibility of stents and surgical implant-devices. Based on the experimental  
data, one of the most recent suggestions is to use an amphiphilic polyurethane  
coating on stents (see e.g., De Scheerder et al.: Biocompatibility of biodegradable  
50 and non-biodegradable polymer coated stents in porcine peripheral arteries.  
*Cardiovasc. Intervent. Radiol.* 18:4, Jul-Aug. 1995, pp.227-32).

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Another approach is based on a discovery made by Chapman in the late 1970's [ See e.g., Chapman, D., et al.: Biomembranes as models for polymer surfaces. *Biomaterials*. Vol. 7, July 1986, pp. 121-5, 126-31 and 252-8; Durrani, AA, Hayward, JA and Chapman, D : Biomembranes as models for polymer surfaces II; The syntheses of reactive species for covalent coupling of phosphorylcholine to polymer surfaces. *Biomaterials*, 7:2, 1986 Mar, pp. 121-5; Hall, B., et al.: Biomembranes as models for polymer surfaces. *Biomaterials*. Vol. 10, May 1989, p.219-224; and Hayward, JA, et al.: Biomembranes as models for polymer surfaces IV; ESCA analyses of a phosphorylcholine surface covalently bound to hydroxylated substrates. *Biomaterial*, 7:4, 1986 Jul. pp. 252-8], who observed that intact biological membranes are highly successful in preventing inappropriate blood clotting reactions. He went on to show that the phosphorylcholine head group is essential in imparting biocompatibility to the phospholipids in the cell-membrane. Some of the most promising and successful attempts of designing biocompatible coatings to date, try to harness these properties: by covalently binding a phosphorylcholine-group to a metal or polymer they attempt to mimic the external surface of biomembranes.

#### 35 Disclosure of the Invention

The present invention is based on a different approach. Instead of coating the stent with polyurethane or any of the other polymers cited above, according to the present invention, a coating of a poly-hydroxy methacrylate derivative is applied to a metallic stent which results in a highly biocompatible and thromboresistant coating for said stents.

More particularly, according to the present invention there is now provided a hemo-compatible, restenosis-inhibiting metallic stent, comprising a coating of a poly-hydroxy methacrylate derivative.

The term poly-hydroxy methacrylate derivative, as used herein, is intended to include hydroxy, alkoxy, and dihydroxy, i.e. glycol derivatives.

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More specifically, the present invention provides a hemo-compatible, restenosis-inhibiting metallic stent, comprising a coating of a poly-hydroxy methacrylate derivative selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof.

In another aspect of the present invention there is now provided a process for producing hemo-compatible, restenosis inhibiting metallic stents including the steps of:

- (a) coating a metallic stent with a liquid which contains a hydroxymethacrylate derivative selected from the group consisting of 2-hydroxyethyl-methacrylate; hydroxyethoxyethyl methacrylate, hydroxydiethoxyethyl methacrylate, methoxyethyl methacrylate, methoxyethoxyethyl methacrylate, methoxydiethoxyethyl methacrylate, ethylene glycol dimethacrylate and mixtures thereof;
- (b) polymerization of said 2-hydroxy-methacrylate derivative into a polyhydroxymethacrylate derivative selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof;
- (c) cleaning the stent after polymerization to extract any remaining residues;
- and
- (d) drying the same.

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The present invention also provides a process for producing  
10 hemo-compatible bioactive restenosis inhibiting metallic stents, comprising the  
steps of:

- 15 a) coating a metallic stent with a liquid which contains poly-hydroxyethylmethacrylate in liquid form;
- b) cleaning the stent to extract any remaining residues; and
- c) drying the same.

20 **Summary of the invention**

Unlike the approach pioneered by Chapman (*Ibid*), the present invention does not aim at mimicking the cell-membrane directly. Rather, the aimed-for biocompatibility is achieved by applying a coating of a poly-hydroxymethacrylate to the metallic surface of a stent. Current uses of 2-hydroxyethyl-methacrylate (hereinafter referred to as HEMA) or its polymer (hereinafter referred to as PHEMA) include adhesives, artificial nails, lacquers, cosmetic compositions, UV-inks and soft lens applications. Surfaces of plastic devices are modified with PHEMA. Furthermore, it is also used as an anti-adhesive to prevent cell attachment in cell cultures, and as an inducer of trabecular bone in dental implants. As such, its non-toxicity and usefulness in medical and biological applications is well-documented.

According to the present invention poly-HEMA is used as a biocompatigenic coating for metal stents. This PHEMA coating renders the stents biocompatible by covering the metallic surface with a uniformly distributed layer of strongly polar and hence hydrophilic groups. As stated hereinbefore, in addition to PHEMA, there are other acrylic-type polymers which are poly-hydroxymethacrylate derivatives and which are similar in general structure to PHEMA:

45 Among these derivatives are poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), and poly

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(ethylene glycol dimethacrylate) (PEGDMA). The use of all these polymers and combinations thereof as coating on metallic stents is part of the present invention, although the invention will now be more specifically described with reference to the preferred PHEMA coating, it being understood that the description with regard to PHEMA is also applicable to said other polymeric coatings.

In a first preferred embodiment of the present invention the polymerization of the HEMA takes place directly on the metallic surface of the stent.

In a second preferred embodiment of the present invention the HEMA is polymerized partly before it comes to the surface of the stent.

In U.S. Patent 5,679,400 there is described a method for providing a therapeutic substance into a body lumen which involves providing a stent and applying to the stent a solution which includes a solvent, a polymer dissolved in the solvent and a therapeutic substance dispersed in the solvent. The polymers described in said patent include bioabsorbable polymers such as poly(lactic acid), poly(lactide-co-glycolide) and poly(hydroxybutyrate-co-valerate) and biostable polymers such as polyurethanes, silicones, polyesters, vinyl homopolymers and copolymers, acrylate homopolymers and copolymers, polyethers and cellulosics, however said patent does not teach or suggest the specific use of a coating of a polyhydroxymethacrylate derivative to a stent in the substantial absence of a therapeutic component in order to provide restenosis-inhibiting properties to said stent and the only acrylate polymer mentioned in said patent is an ethylene-methyl methacrylate copolymer, listed as one among tens of other named polymers.

Several explanations may be offered for the biocompatigenic nature of PHEMA. One possibility is that the strongly hydrophilic nature of the outside layer of PHEMA attracts a dense water-coat, thus preventing blood-corpuscles to come into direct contact with the stent, an event that normally triggers the thrombogenic reaction (see, e.g., Binderman, I., et al., Grafts of HTR Polymer versus Kiel Bone in Experimental Long Bone Defects in Rats, ASTM, PA 19103).

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Alternatively, it may be the case that polar PHEMA coating attracts the polar moiety on circulating phospholipids which then precipitate under the form of a lipid bilayer. In this instance, biocompatibility would again be a consequence of mimicking the thromboresistance of cell-membranes. If this latter hypothesis turns out to be correct, it underscores the possibility of self-assembly and hence self-repair of the very factor that induces biocompatibility. This is an extremely desirable property for a stent, especially in locations where there are considerable shear forces due to strong blood-circulation, such as heart and main arteries. In addition, PHEMA coated stents prevent adverse cell reaction of the injured site, cell growth, and restenosis.

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Whatever the explanation, it has now been found that coating of the metallic surface of stents with PHEMA results in the creation of a stable and highly biocompatible coating which makes the stent thromboresistant and prevents the deposition of protein and adverse vessel-wall reactions, thus vastly increasing their value in surgical procedures.

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Thus, the present invention enables the prevention or minimization of restenosis that is evident in some cases with the introduction of metallic stents, by providing hemo-compatible bioactive restenosis-inhibiting metallic stents.

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2-Hydroxyethyl methacrylate (HEMA) can be polymerized into poly-HEMA (PHEMA), which is a polymer exhibiting a strongly polar character. PHEMA shows minimal bacterial or cell binding but excellent cell biocompatibility, no protein deposition and no blood clotting. This means that blood plaques which might trigger the development of a potentially fatal thrombus will not be formed. As there is little or no bacterial adhesion, the risk of infections is minimized. PHEMA is a coating which can be used on metal based stents, and which makes these stents biocompatible. The stents can be made of stainless steel, Ti-based alloys, shape memory alloys or any other metal, eventually in combination with synthetic or biological materials. The stents are coated with the hydrophilic HEMA-monomer, which is then polymerized by using dielectric heating, UV light, electron-beam

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radiation, gamma-radiation, ozone initiation, X-rays, lasers, visible light, thermal  
10 cure or any other means. Thus, said polymerization can be initiated by at least  
one of photopolymerization, ionic-polymerization, and chemical-polymerization.

15 After the polymerization procedure, the stent is placed in hot or boiling liquid,  
e.g. water to remove the remaining monomers. Such stents find applications in e.g.  
vascular, endo-esophageal and urological stents, as well as for coronary artery  
bypass surgery or the repair of aneurysms, etc. .

20 In general, the procedure for preparing coated stents according to the present  
invention is as follows:

25 A stock solution is prepared by dissolving the 2-hydroxyethyl methacrylate  
(HEMA), formula  $C_6H_{10}O_3$ , CAS Number 868-77-9, in ethanol. Other possible  
solvents are dimethyl sulfoxide (DMSO), propanol, glycerol, ethylene glycol,  
cyclohexanol, toluene and dimethyl formamide (DMF). It is preferable to use the  
HEMA in an as pure as possible form, typically better than 98.4%. Typical  
30 solutions are made by dissolving 120 mg HEMA in 1 ml 95% ethanol. The  
dissolving process is helped by shaking the solution and a storage at e.g. 37°C for  
12 hrs. A separation of undissolved material can be reached by centrifuging at e.g.  
2500 rpm for 30 min. Further dilution with ethanol can be used to produce coatings  
35 of various thickness. Polymerization is lightly inhibited by trace amounts of an  
inhibitor such as the methyl ether of hydroquinone (MEHQ). MEHQ should be  
present in a concentration within the range of 150 to 300 ppm, preferably 200 ppm.  
The HEMA can be modified by the addition of a cross linking agent such as  
40 triethyleneglycol dimethacrylate, which comprises between about 0.1 and 6% of the  
HEMA, preferably 5%. Alternatively, tetraethylenglycol dimethacrylate,  
diethyleneglycol dimethacrylate and monoethyleneglycol dimethacrylate can be  
45 used. A combination of these diesters can also be used.

50 After wetting the stents with the described solution, they can be air dried in a  
e.g. sterile environment (sterile lamina flow hood), or when inhibitors are applied,  
the polymerization can take place by means of a dielectric furnace, UV light or

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controlled temperature chamber. The heating provides sufficient free radical activity to overcome the effect of the inhibitor, resulting in polymerization of the coating. The heating step is, e.g. about 1.5 minutes in duration in a dielectric furnace when the upper electrode is positioned about 5 mm above the stent. In order to remove any remaining HEMA monomer and/or traces of the inhibitor after the polymerization step, the stent is boiled in water for about 2 to 3 minutes after cooling down. This procedure will leach out any remaining HEMA monomer and/or inhibitor. After boiling, the stents can be dried at a slightly higher temperature. 2-hydroxyethyl methacrylate can be applied directly to the stent or with the help of a primer such as silanes.

In order to further improve the biocompatibility, the surface modification by selective alkaline hydrolysis was studied. It was found that the thickness of the modified layer can be influenced by the reaction temperature, NaOH concentrations and reaction time.

Using at least 30% NaOH, short reaction times and temperatures of at least 90° C, coatings with carboxylic groups in the surface layer were prepared. This method can be used for obtaining hydrophilic medical coatings with further improved properties and further increased biocompatibility.

The scope of the invention includes the coating with a poly-hydroxymethacrylate derivative of all metallic surfaces of stents of all types, as well for only metallic stents and for the coating of stents formed from the combination of metal with synthetic or biologic tissues.

#### 40 Description of Preferred Embodiments

While the invention will now be described in connection with certain preferred embodiments in the following examples so that aspects thereof may be more fully understood and appreciated, it is not intended to limit the invention to these particular embodiments. On the contrary, it is intended to cover all alternatives, modifications and equivalents as may be included within the scope of the invention as defined by the appended claims. Thus, the following examples which include preferred embodiments will serve to illustrate the practice of this invention, it being understood that the

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particulars shown are by way of example and for purposes of illustrative discussion of  
10 preferred embodiments of the present invention only and are presented in the cause of  
providing what is believed to be the most useful and readily understood description of  
formulation procedures as well as of the principles and conceptual aspects of the  
invention.

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**Example 1**

1. A stock solution is prepared by dissolving 120 mg 2-hydroxyethyl  
methacrylate (HEMA), formula C<sub>6</sub>H<sub>10</sub>O<sub>3</sub>, CAS Number 868-77-9, in 1 ml 95%  
20 ethanol. It is preferable to use the HEMA in an as pure as possible form, typically  
better than 98.4%.

2. The dissolving process is helped by shaking the solution for 1 hr. and storing  
at 37 °C for 12 hr.

25 3. A separation of undissolved material is then reached by centrifuging at 2,500  
rpm for 30 min.

4. Polymerization is lightly inhibited by utilizing trace amounts of an inhibitor (2  
30 drops) and the methyl ether of hydroquinone (MEHQ) is utilized for this purpose.

5. The Palmaz-Schatz stent and a Wiktor stent were used in this particular  
example. Other stents have been used in other tests.

35 6. The stents were thoroughly cleaned using laboratory detergents, and  
washed in warm water.

7. The stents were left to air dry in a sterile environment (sterile lamina flow  
hood).

40 8. The stents were then wetted with the solution by dipping them in the solution  
to the point where their entire surface was submerged in the liquid.

9. Using a specially designed lever, the stents were lifted out of the solution at  
45 a rate of 1 mm/sec. This facilitated the uniformity of the coat.

10. The stents were left to air dry in a sterile environment (sterile lamina flow  
hood).

50 11. Steps 8-10 were repeated 4 times in order to get the appropriate coating  
thickness.

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10        12. The stents were moved to a UV light chamber and radiated for an additional 10 min. The stents were then placed in the chamber in a way that all sides of the stent were no more than 3 cm away from each lamp.

15        13. In order to remove any remaining HEMA monomer and/or traces of the inhibitor after the polymerization step, the stent was boiled in water for about 2 to 3 minutes after cooling down.

20        14. After boiling, the stents were dried at a slightly higher temperature.

25        15. The stents were then placed on an angioplasty balloon and were inflated to 85% of their range.

30        16. The stents were weighed and examined under a scanning microscope to determine the uniformity of the coat and its attachment to the stent surface.

35        17. The stents' surface appeared to be completely covered and to a sufficient level of uniformity. Coating adhesion remained intact even under severe stress.

Example 2

40        1. A stock solution was prepared by dissolving 120 mg poly-hydroxyethyl methacrylate (PHEMA) IN 1 ML 95% ethanol. It is preferable to use the PHEMA in an as pure as possible form, typically better than 98.4%.

45        2. The dissolving process was helped by heating the solution to 75 °C and shaking the solution for 1 hr.

50        3. A separation of undissolved material was reached by centrifuging at 3.g. 2500 rpm for 30 min.

55        4. The Palmaz-Schatz stent and a Wiktor stent were used in this particular example. Other stents have been used in other tests.

60        5. The stents were thoroughly cleaned using laboratory detergents and washed in warm water.

65        6. The stents were left to air dry in a sterile environment (sterile lamina flow hood).

70        7. The stents were then wetted with the solution by dipping them in the solution to the point where their entire surface was submerged in the liquid.

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8. Using a specially designed lever, the stents were lifted out of the solution at a rate of 1 mm/sec. This facilitated the uniformity of the coat.

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9. The stents were left to air dry in a sterile environment (sterile lamina flow hood) for 15 min.

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10. Steps 7-9 were repeated 4 times in order to obtain the appropriate coating thickness.

11. The stent was boiled in water for about 2 to 3 minutes.

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12. After boiling, the stents were then air-dried at a slightly higher temperature.

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13. The stents were then placed on an angioplasty balloon and were inflated to 85% of their range.

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14. The stents were weighed and examined under a scanning microscope to determine the uniformity of the coat and its attachment to the stent surface.

15. The stents' surface appeared to be completely covered and to a sufficient level of uniformity. Coating adhesion remained intact even under severe stress.

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It will be evident to those skilled in the art that the invention is not limited to the details of the foregoing illustrative examples and that the present invention may be embodied in other specific forms without departing from the essential attributes thereof, and it is therefore desired that the present embodiments and examples be considered in all respects as illustrative and not restrictive, reference being made to the appended claims, rather than to the foregoing description, and all changes which come within the meaning and range of equivalency of the claims are therefore intended to be embraced therein.

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**Claims**

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**WHAT IS CLAIMED IS:**

10. 1. A hemo-compatible, restenosis-inhibiting metallic stent, comprising a coating of a poly-hydroxy methacrylate derivative.
15. 2. A hemo-compatible, restenosis-inhibiting metallic stent according to claim 1, comprising a coating of a poly-hydroxy methacrylate derivative selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof.
20. 3. A process for producing hemo-compatible, restenosis inhibiting metallic stents comprising the steps of:
  25. (a) coating a metallic stent with a liquid which contains a hydroxymethacrylate derivative selected from the group consisting of 2-hydroxyethyl-methacrylate; hydroxyethoxyethyl methacrylate, hydroxydiethoxyethyl methacrylate, methoxyethyl methacrylate, methoxyethoxyethyl methacrylate, methoxydiethoxyethyl methacrylate, ethylene glycol dimethacrylate and mixtures thereof;
  30. (b) polymerization of said 2-hydroxy-methacrylate derivative into a polyhydroxymethacrylate derivative selected from the group consisting of poly-hydroxyethylmethacrylate (PHEMA), poly (hydroxyethoxyethyl methacrylate) (PHEEMA), poly (hydroxydiethoxyethyl methacrylate) (PHDEEMA), poly (methoxyethyl methacrylate) (PMEMA), poly (methoxyethoxyethyl methacrylate) PMEEMA, poly (methoxydiethoxyethyl methacrylate) (PMDEEMA), poly (ethylene glycol dimethacrylate) (PEGDMA), and mixtures thereof; and
  35. (c) cleaning the stent after polymerization to extract any remaining residues.
40. 4. The process of claim 3 wherein the stent is cleaned in warm water.

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5. The process of claim 3 comprising the additional step of adding a cross  
linking agent.
10. The process of claim 5, wherein said cross linking agent is present in an  
amount of about 0.1% to 6% weight relative to the weight of the  
2-hydroxyethyl-methacrylate monomer.
15. The process of claim 3 wherein the stent is first treated with a primer.
20. The process of claim 3 wherein the stent is made from a metal in  
combination with a polymer.
25. The process of claim 3 wherein the stent is made from stainless steel.
30. The process of claim 3 wherein the stent is made from a Ti-based alloy.
35. The process of claim 3 wherein the stent is made from a shape memory  
alloy.
40. The process of claim 3 wherein the polymerization is carried out at  
atmospheric pressure.
45. The process of claim 3 wherein the polymerization is carried out by  
dielectric heating.
50. The process of claim 3 wherein the polymerization is carried out by  
induction heating.
55. The process of claim 3 wherein the polymerization is initiated by at least  
one of photopolymerization, ionic-polymerization, and chemical-polymerization.
60. The process of claim 3 wherein the polymerization is carried out at  
elevated pressures.
65. The process of claim 3 wherein the polymerization is carried out at  
temperatures in the range of 150°C to 230°C.
70. The process of claim 5, wherein said cross linking agent is methacrylic  
diester of ethyleneglycol.

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19. The process of claim 18, wherein said methacrylic diester of ethyleneglycol  
10 is selected from the group consisting of:

- (a) tetraethyleneglycol dimetacrylate,
- (b) triethyleneglycol dimethacrylate,
- (c) diethyleneglycol dimethacrylate,
- (d) monoethyleneglycol dimethacrylate, and
- (e) mixtures thereof.

20. The process of claim 3, wherein said poly-hydroxyethylmethacrylate  
comprises a copolymer of monomeric 2-hydroxyethyl-methacrylate.

21. The process of claim 20, wherein said coating contains a cross linking  
agent.

25. The process of claim 3 wherein NaOH is added before said polymerization  
step.

30. The process of claim 22, wherein said at least 30% NaOH is used.

35. The process of claim 22, wherein said polymerization is effected at a  
temperature of at least 90°C.

40. The process of claim 3, comprising diluting said  
45. poly-hydroxyethylmethacrylate containing liquid in order to obtain different coating  
thicknesses.

50. A process for producing hemo-compatible bioactive restenosis inhibiting  
metallic stents, comprising the steps of:

- a) coating a metallic stent with a liquid which contains  
poly-hydroxyethylmethacrylate in liquid form;
- b) cleaning the stent to extract any remaining toxic residues; and
- c) drying the same.

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## INTERNATIONAL SEARCH REPORT

International Application No  
PCT/IL 99/00376

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 7 A61L31/10

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
IPC 7 A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	CA 2 226 129 A (HUELS CHEMISCHE WERKE AG) 3 July 1998 (1998-07-03) page 15, line 19 -page 16, line 14 page 20, line 23 -page 21, line 3 ----	1-12,15, 20,21,26
X	WO 96 25897 A (MENLO CARE INC) 29 August 1996 (1996-08-29) claims 1,4,6,14 ----	1-12,15, 20,21,26
A	EP 0 574 880 A (UNITED STATES SURGICAL CORP) 22 December 1993 (1993-12-22)  page 4, line 46 - line 55 example 4 -----	1-3,5,6, 15, 18-21,26

Further documents are listed in the continuation of box C.

Patent family members are listed in annex.

\* Special categories of cited documents :

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- "E" earlier document but published on or after the international filing date
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- "D" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

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"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

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Date of the actual completion of the international search

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Information on patent family members

International Application No
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## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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(60) Parent Application or Grant <b>SCIMED LIFE SYSTEMS, INC. [/]; () YANG, Dachuan [/]; () WANG, Lixiao [/]; () ANDERSON, William, E., II; ()</b>		

(54) Title: DRUG DELIVERY DEVICE FOR STENT

(54) Titre: SYSTEME D'ADMINISTRATION DE MEDICAMENTS POUR STENT

(57) Abstract

A device adapted for mounting on a stent, the device comprising a sheath being made of polymeric material that includes drugs such as pharmaceutical agent(s) or radioactive agent(s) for delivery to an implant site. The sheath includes a main body of a generally tubular shape, and may include mounting means for attaching same to the stent. The device may have a slit therein, and may comprise a helical coil, a cylinder or any other suitable shape or design which fits a particular stent. The sheath may include a coating or coatings thereon containing drugs, surgical adhesives or a combination thereof.

(57) Abrégé

L'invention concerne un dispositif conçu pour être monté sur un stent. Ce dispositif comprend une gaine en matériau polymère contenant des médicaments, par exemple un ou plusieurs agent(s) pharmaceutiques, devant être administrés sur le site d'implantation. Cette gaine comprend un élément principal de forme sensiblement tubulaire et peut comprendre des moyens de fixation permettant de la fixer sur le stent. Le dispositif peut comprendre un fente ainsi qu'un enroulement hélicoïdal, un cylindre ou toute autre forme ou structure adaptée à un stent particulier. La gaine peut en outre comprendre une ou plusieurs couches de revêtement contenant des médicaments, des adhésifs chirurgicaux ou une combinaison des deux.

